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**Contrast-enhanced CT texture parameters as predictive markers of high-risk urodynamic features in adult patients with spina bifida**

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The authors have nothing to disclose

## **Abstract**

### Objective

to investigate computed tomography (CT) texture analysis of the bladder wall as a predictor of urodynamics findings in adult patient with spina bifida.

### Methods

A single-center prospective trial was conducted from March 2015 to March 2017 including all consecutive adult spina bifida patients seen for urodynamic testing. A contrast-enhanced abdominal CT was systematically performed in all patients during the same visit. Texture features of the bladder wall related to the gray-level histogram and gray-level co-occurrence were evaluated on CT images. Multivariate analysis was performed to identify independent predictors of poor bladder compliance (PBC) and detrusor overactivity (DO) among clinical and texture parameters.

### Results

Fourty patients were included. The Lasso penalized logistic regression analysis identified two texture parameters as potential predictors of poor bladder compliance: Skewness (coefficient weight, -1.81) and S.1.1.SumVarnc (coefficient weight, -3.52). Multivariate Logistic regression analysis confirmed skewness (OR (CI 95%) = 0.40 (0.14, 0.97),  $p = 0.04$ ) as an independent predictor of PBC. The Lasso penalized logistic regression analysis identified one texture parameters as potential predictor of DO: Kurtosis (coefficient weight, -3.52). which was confirmed in multivariate logistic regression analysis (OR (CI 95%) = 1.12 (1.01, 1.55),  $p = 0.02$ ).

### Conclusion

Our findings demonstrate that CT texture analysis of the bladder wall might be an interesting tool to identify spina bifida patients with high risk urodynamic features.

## Introduction

Spina bifida is a birth defect originally defined as an incomplete closure of the neural tube in the caudal region resulting in protrusion of part or all of the content of the spinal canal through this dorsal defect [1]. Spina bifida is the most common congenital cause of neurogenic bladder with an incidence of 1/10,000 births in developed countries [1-2]. Neurogenic lower urinary tract dysfunction (NLUTD) is present in more than 90% of spina bifida patients and carries a high-risk of upper urinary tract damage [3]. For that reason, most guidelines recommend to repeat urodynamics over follow-up to monitor bladder pressure and tailor therapeutic management [4]. However, repeat urodynamics cause a severe burden to spina bifida patients due to its invasiveness and are costly for the healthcare systems. Several non-invasive alternatives to urodynamics have been evaluated over the past decade [5] but, so far, none has been deemed reliable enough to be implemented in daily practice. In the last decade, there has been an increasing interest in the analysis of quantitative information from medical images to improve the performance and usefulness of imaging. Textural analysis relies on objective computer-assisted measurements and explore the spatial variations of signal intensity in imaging [6]. Numerous published articles have shown the ability of texture analysis algorithms to extract information from various imaging modalities in several fields [7]. We aimed to investigate computed tomography (CT) texture analysis of the bladder wall as a predictor of urodynamics findings in adult patient with spina bifida.

## Materials and Methods:

### Study design

From March, 2015 to March, 2017 all adult spina bifida patients seen at the national referral center for spina bifida were offered a routine urological evaluation whether they had urological complaints or not. All consecutive patients undergoing urodynamics for the assessment of their lower urinary tract function were enrolled in a prospective study (ClinicalTrials.gov Identifier: NCT02852317). All study materials were reviewed and approved by the local Independent Ethics Committee, and all patients provided written informed consent. Patients were excluded if they had an ongoing symptomatic urinary

tract infection, or a history of augmentation cystoplasty or urinary tract malignancy. The following variables were collected for each patient: demographics, past medical history, physical examination, bladder management (self-catheterization vs. spontaneous voiding) bladder diary data, urine culture, types of spinal dysraphism (open vs. closed), ongoing and previous bladder medications (anticholinergics, beta-3 agonists,...), and history of intradetrusor botulinum toxin injections. The type of spinal dysraphism (open vs. closed) was defined based on previous spine imaging and operative reports and on a Magnetic Resonance Imaging (MRI) of the spine performed at the time of the first visit for every patients. The sensory-motor level of neurological impairment was categorized as sacral, lumbar or thoracic.

#### Urological assessment

At the first visit, lower urinary tract function was systematically assessed regardless of the presence or not of lower urinary tract symptoms (LUTS). Each single patient during his/her first visit to the center was seen in clinics by a urologist. The urologist's assessment included: history of past urological surgery, bladder management (clean-intermittent catheterization (CIC) vs. spontaneous voiding), urinary incontinence defined as any urine leakage reported by the patient at least once a week or evidenced during clinical examination or by the use of any pads, oral anticholinergics intake (yes vs. no). All patients underwent a morphological evaluation of the urinary tract using abdominal computerized tomography (CT, see details below) as part of their initial urological assessment.

#### Urodynamic evaluation

All patients seen at the French referral center for spina bifida were offered a urodynamic study at their first visit even though they came to the center for a non-urological issue and were completely asymptomatic from the urological standpoint. Standard filling cystometry using saline was done with patients in the supine position using a 7Fr to 10Fr double lumen urethral cystometry catheter and a rectal balloon catheter according to the International Continence Society (ICS) standards [8]. Anticholinergic therapy was discontinued at least one week before urodynamic evaluation. Filling cystometry was

then performed at a rate of 20 mL/min with saline. Neurogenic detrusor overactivity (NDO) was defined in accordance with the recent standardization of terminology report by the ICS as a urodynamic observation characterized by involuntary detrusor contractions during the filling phase which may be spontaneous or provoked in the setting of a clinically relevant neurologic disease [9]. The following urodynamics data, defined according to the ICS guidelines [8], were also collected: cystometric capacity (CC, ml), volume at first sensation of bladder filling (ml), volume at first uninhibited detrusor contraction if any (ml), bladder compliance calculated manually from the traces (ml/cmH<sub>2</sub>O), maximum detrusor pressure (MDP, cmH<sub>2</sub>O). Poor bladder compliance was defined as bladder compliance < 20 ml/cmH<sub>2</sub>O according to the ICS standardization report [8].

#### Quantitative computed tomography Texture analysis of bladder wall CT technique

All patients underwent contrast-enhanced CT. Patients were asked to present with a full bladder for the CT. To obtain three representative images per patient, regions of interest (ROIs) were defined in the coronal plane at three levels through the craniocaudal dimension of the bladder corresponding to approximately the upper third, center and lower third of the organ (figure 1). The area and position of the ROI for each level was kept constant.

#### CT Texture Analysis

Each image was collected and stored in the original digital imaging and communication in medicine (DICOM) format. Images were anonymized. These images were then transferred to an independent workstation for lesion segmentation by using ImageJ software (National Institutes of Health, <http://rsbweb.nih.gov/>). For each image a ROI was manually drawn slightly on enhanced image. Prior to analysis, CT image intensities were normalized between  $\mu \pm 3s$ , where  $\mu$  was the mean value of gray levels inside the region of interest and  $s$  was the standard deviation. This normalization procedure has been shown to minimize inter-scanner effects in MRI texture analysis and is presumed to also reduce inter-scanner effects in other modalities such as CT (figure 2). Texture

features related to the gray-level histogram and gray-level co-occurrence (GLCM), were evaluated using MaZda, version 4.6 (P.M. Szczypiński, Institute of Electronics, Technical University of Lodz, Poland).

### Statistical analysis

We restricted our analysis to patient-level means for each feature and for each set of contours. Quantitative variables were described as means with standard deviation or medians with minimum-maximum and categorical variables as percentages. Multivariate analysis was performed to identify independent predictors of poor bladder compliance and detrusor overactivity among clinical and texture parameters. To take into consideration the correlation between the estimates of each texture parameter and the small number of events, a multivariate L1 (least absolute shrinkage and selection operator—Lasso) penalized logistic regression model was built in order to select texture parameters. The regularization parameter was determined by using tenfold cross-validation. The Lasso method allows variable selection by shrinking down to zero coefficient weights for variables non-related to the outcome. Variables with non-zero coefficients were selected as potential predictors of outcome and integrated into a multivariable logistic regression analysis, in order to estimate associated hazard ratios (HR) and their 95% confidence intervals (CI 95%). For each texture parameter predictor of outcome, an additional analysis was performed to determine the optimal threshold dividing out patients with good and poor prognosis, based on the threshold with the highest Youden index using non-parametric test. All statistical analyzes were performed using R software (R Foundation for Statistical Computing, Vienna, Austria) and STATA 13.0 (College Station, TX).

## Results

### Patient characteristics

Forty patients were enrolled over the study period. The patients' characteristics are summarized in supplementary table 1. The mean patients' age was 37.7 years and there

was 52.5% and 48.5% of male and female patients respectively. The majority of patients were self-catheterizing (70%) and the predominant neurological level was lumbar (79%). The mean maximum voided volume on the voiding diary was 419.7 ml. Eleven patients had signs of upper urinary tract damage on imaging (27.5%): hydronephrosis in eight patients (20%), renal scarring in two patients (5%) and renal atrophy in two patients (5%). The urodynamic findings are shown in supplementary table 2. The mean CC, MDP and volume at first sensation of bladder filling were 419.7 mL, 24.4 cmH<sub>2</sub>O and 225.7 mL respectively. There were 15 patients with poor bladder compliance (37.5%) and 15 patients with DO (37.5%).

#### Poor bladder compliance analysis

The Lasso penalized logistic regression analysis identified two texture parameters as potential predictors of poor bladder compliance: Skewness (coefficient weight, -1.81) and S.1.1.SumVarnC (coefficient weight, -3.52). Two clinical parameters also highlighted non-zero coefficient weights: age (coefficient weight, -1.43), and type of spinal dysraphism (coefficient weight 3.55). Multivariate Logistic regression analysis confirmed skewness (OR (CI 95%) = 0.40 (0.14, 0.97),  $p = 0.04$ ), and age (HR (CI 95%) = 0.96 (0.92, 0.995),  $p = 0.02$ ) as independent predictors of poor bladder compliance (table 1). When dichotomized at the optimal threshold, skewness under  $-0.417$  was significantly associated with high risk of poor bladder compliance ( $p = 0.02790$ ).

#### Detrusor overactivity

The Lasso penalized logistic regression analysis identified one texture parameters as potential predictor of detrusor overactivity: Kurtosis (coefficient weight, -3.52). Four clinical parameters also highlighted non-zero coefficient weights: age (coefficient weight, -1.42), type of spinal dysraphism (coefficient weight 3.57), neurological level (coefficient weight 3.57) and male gender (coefficient weight 1.43). Multivariate Logistic regression analysis showed that only kurtosis (OR (CI 95%) = 1.12 (1.01, 1.55),  $p = 0.02$ ) was an independent predictor of detrusor overactivity (table 2). When dichotomized at the



optimal threshold, kurtosis under 1.48 was significantly associated with high risk of detrusor overactivity ( $p= 0.0212$ )

## Discussion

Spina bifida is the most common congenital cause of NLUTD [2]. Spina bifida patients are subject to severe NLUTD which often have very specific features with high prevalence of acontractile detrusor, poor bladder compliance and intrinsic sphincter deficiency [3]. Until now, initial assessment and follow-up of spina bifida NLUTD has been relying heavily upon urodynamics as being the only exam able to properly identify and characterize NLUTD, with some literature showing correlations with the risk of upper urinary tract deterioration [10-11]. However, urodynamics have its cons including the invasiveness of urethral catheterization, discomfort of the exam for the patient, cost to healthcare system and significant variability/risk of artifacts [12]. Hence, several alternatives to urodynamics have been investigated over the past two decades such as urinary markers or ultrasonographic parameters [5]. To our knowledge this study is the first to explore CT texture analysis as a predictor of urodynamic findings in spina bifida patients or in any other neurologic patients. We found that some CT texture parameters were significantly associated with high risk urodynamic features such as poor bladder compliance suggesting that CT texture analysis of the bladder wall might be an alternative to urodynamics for spina bifida patients in selected situations.

Image texture analysis can be described as a wide range of techniques for quantification of gray-level patterns and pixel inter-relationships within an image. In other terms, it can be considered as a mathematical representation of image features that can be characterized in words. Texture analysis relies on a process that includes six steps: 1) images acquisition, 2) region of interest ROI definition, 3) ROI preprocessing, 4) feature extraction, 5) feature selection and 6) classification. However, none is specific and many parameters can vary in each step [6-7, 13]. Therefore, collaborative efforts are mandatory to develop and validate protocols for each step. First, a global effort towards standardization of imaging is necessary. This effort requires standardization not only for image acquisition protocols, but also for volume of interest identification and features

extractions. There is also a fundamental need that the medical and scientific communities design studies to enable the translation of imaging biomarkers from "bench" to clinical practice [6-7, 13]. Though the use of retrospectively collected data is necessary to develop, test and evaluate texture analysis as an imaging biomarker, the risk to select significant features by chance and overfitting is major. Therefore, prospective studies to identify promising features from texture analysis with external validation in multicentric cohorts are necessary [13-14]. Finally, efforts should be directed towards the determination of the mechanisms beyond the correlations observed between clinical findings and corresponding texture features [13-14].

Our results suggest the potential usefulness of quantitative measures from texture analysis to detect detrusor overactivity or poor bladder compliance in spina bifida patients. We found skewness and kurtosis be statistically associated with the presence of poor bladder compliance and detrusor overactivity. These quantitative measures do not have simple qualitative description, but reflect subtle patterns of dependencies in the image [15]. Skewness is a measure of histogram asymmetry; a zero value indicates a symmetrical distribution around the mean. We speculate that in fibrotic, thickened poorly compliant bladders the resulting histograms from ROIs are likely to be more skewed compared with normal compliance bladder with less heterogeneous cellular density [15]. The correlation between fibrosis and skewness that has been demonstrated in other conditions would support this idea of skewness indicating fibrosis responsible of decreased bladder compliance [16]. Kurtosis is another histogram-based method which measures histogram flatness. The increased kurtosis associated with detrusor overactivity could reflect the increase intensity variation in the bladder wall of these patients that might indicate microstructural changes [15].

One of the points of strength of our series was the systematic CT performed in all spina bifida patients at the first visit to the national referral center. While our findings suggest that CT texture analysis may provide valuable information regarding NLUTD, the exposure to ionizing radiation associated with the use of CT in this young patient population shall raise concerns [17-18] and prevent to advocate for the use of repeat CT as an alternative to repeat urodynamics. However, CT is commonly used in the

neurourological management of spina bifida patients in the context of urinary tract infections or to detect urolithiasis [4, 19-20]. Abdominal CT are also frequently performed for other purposes in spina bifida patients, for instance for ventriculo-peritoneal shunts issues [21]. Hence, rather than pleading for dedicated CT to replace urodynamics in some instances, the promise of CT texture analysis if confirmed might support the analysis of data from existing CT performed for other purposes to draw information regarding NLUTD. Such a tool might be of interest as part of multimodal neurourological follow-up protocols in spina bifida patients. Texture analysis can also be performed using magnetic resonance imaging (MRI). Future studies exploring the value of MRI feature parameters to predict high risk urodynamic features might open up another way to use radiomics as an alternative to urodynamics divested from the radiation exposure issue.

Our study has some limitations that should be acknowledged. First, it was a retrospective monocentric study, with a relatively small number of patients. Second, drawing of ROIs was done manually, possibly introducing variability. Third, we performed two-dimensional texture analysis on regions of interest selected from three axial sections rather than three-dimensional analysis, which might allow a more precise evaluation of the picture heterogeneity and also improve reproducibility. However, several studies have shown that use of a single slice is sufficient for sampling and extracting subtle features relevant for clinical application [22]. Fourth, our results were obtained using open access texture analysis software and we cannot extend our conclusions to other software programs. The decision to select detrusor overactivity and poor bladder compliance as the relevant urodynamic outcomes of interest might be called into question as other urodynamic parameters such as Pdetmax or detrusor leak point pressure may have been regarded as valuable alternatives. The bladder condition at the time of the CT was not perfectly standardized which might be regarded as a shortcoming. However, the texture parameters were extracted from the bladder wall images and whether they might be influenced by the degree of bladder filling is unknown. We decided not to include a control group of healthy volunteers to maximize the chance that radiomic differences observed would reflect bladder function differences

rather than differences inherent to the spina bifida condition itself. However, this methodological choice might be considered as a study's flaw. Another possible shortcoming of this study is that we did not include analysis of CT gross morphology data which have never been explored as possible predictors of urodynamic features and might therefore deserve further investigations. The fact that models that learn from data are developed from a single technique and a single classifier selected based on researchers' preference and experience could be regarded as a shortcoming of the radiomics study in general and of our study in particular. Finally, the number of covariates was large compared to sample size. We addressed this issue by using the LASSO penalised regression model, which is suitable for analysis of high dimensional data

## **Conclusion**

Our findings demonstrate that CT texture analysis of the bladder wall might be an interesting tool to identify spina bifida patients with high risk urodynamic features. This suggests that CT texture analysis of the bladder wall might be a non-invasive alternative to urodynamic for spina bifida patients in selected clinical scenarios. Further investigations with new textural analysis and prospective validation of the textural candidates identified in this study and mandatory to develop an accurate and comprehensive multi-functional signature of high-pressure spina bifida bladder in the future. Assessment of the value of CT texture analysis in other neurologic conditions may also be of interest.

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Figure legends

Figure 1: Illustration of lesion delineation



Figure 2: Overview workflow of the method

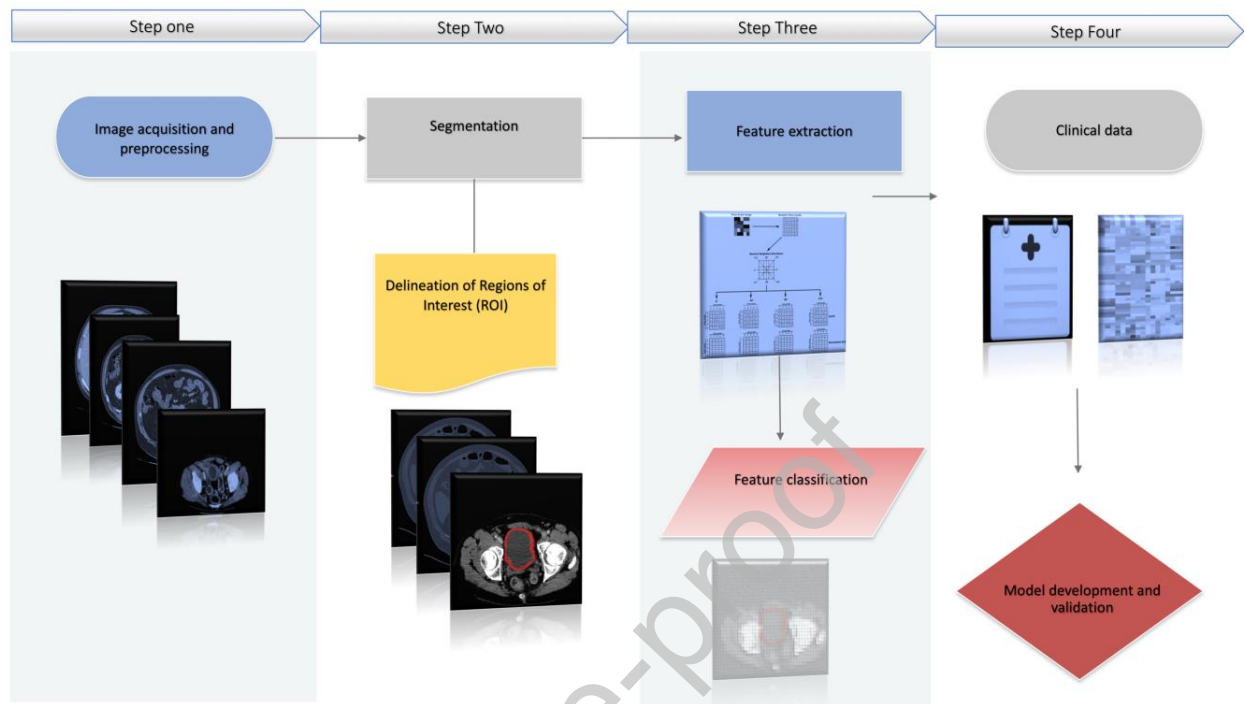




Table 1: Multivariate Logistic proportional hazards regression analyses of texture features and clinical parameters selected by Lasso penalized logistic regression analysis for predicting poor bladder compliance

	<b>Odds-ratio [CI-95%]</b>	<b>p-value</b>
<b>Age</b>	0.96 [0.92-0.99]	0.2
<b>Type of Spinal dysraphism</b>	1.29 [0.29-5.78]	0.73
<b>Skewness</b>	0.41 [0.15-0.98]	0.04
<b>S11sumVarnc</b>	1.00 [0.99-1.01]	0.245

Table 2: Multivariate Logistic proportional hazards regression analyses of texture features and clinical parameters selected by Lasso penalized logistic regression analysis for predicting detrusor overactivity

	<b>Odds-ratio [CI-95%]</b>	<b>p-value</b>
<b>Age</b>	1.01 [0.96-1.06]	0.71
<b>Male gender</b>	1.16 [0.27-5.00]	0.85
<b>Kurtosis</b>	1.12 [1.01-1.55]	0.026
<b>Type of spinal dysraphism</b>	1.00 [0.99-1.01]	0.17